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Sectio	on B - Supplies or Services and Price	es		
ITEM NO 0001	SUPPLIES/SERVICES QUAI	NTITY UNIT Lot	UNIT PRICE	AMOUNT
0001	Non-lethal Weapons Study COST	Lot		
	Sensory Consequences of Electron Plasmas	nagnetic Pulses Emitt	ed by Laser Induced	
	MILSTRIP: M9545004RCR4DH2	;		
			ESTIMATED COST	\$514,175.00
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Page 3 of 24

Section C - Descriptions and Specifications

STATEMENT OF WORK C1 Statement of Work

CLIN 0001 and Option CLIN 0002 shall be in accordance with the Statement of Work attached to this contract.

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Section J - List of Documents, Exhibits and Other Attachments

Exhibit/Attachment Table of Contents

DOCUMENT TYPE	DESCRIPTION	PAGES	DATE
Attachment 1	Statement of Work	10	

### 1. Technical

A) Objectives/Tasks/Concept. Recent advances in directed energy weapons technology suggests that scalable, non-lethal to lethal force systems may be possible. Such a system would be useful in many environments. Two systems currently under development, active denial and pulsed energy (ADS and PEP) offer mainly complementary capacities that could address multiple tasks

These tasks include the The full capability of these directed energy systems (DE) are still being explored. At their current stage of development, each system has clear nonlethal (ADS) and lethal (PEP) capacities suitable to the above tasks. Our experiments will examine the feasibility of PEP as a new generation non-lethal weapon. Pulsed energy can be configured to produce plasmas of exceptionally high energy.

studies described below we will determine the feasibility of using the plasma derived EMP to induce pain suitable to disarm and deter individuals or form barriers to the movement of large hostile groups. If successfully deployed, PEP could complement ADS in situations in which the latter is ineffective, less effective, or prone to countermeasures. Many of the countermeasures that might be envisioned against ADS for opportunities for PEP targeting (via plasma induction or ablation of the defense). Despite these potential advantages, certain special capabilities and features of ADS offer advantages over PEP in many scenarios. Therefore, the systems are complementary.

The efficiency and lethality of PEP weapons systems are straightforward. The non-ballistic, instantaneous properties of DE make precise targeting a straightforward matter of line of sight. Terrific amounts of energy can be delivered over great distances with pinpoint accuracy. However, Potentially, Potentially,

the application of PEP

The pain induced would be relatively

instantaneous, and the duration of pain would be limited to the duration of application Taser-like motor effects are also possible, although these are not investigated in this

proposal.

In a separate application, we have proposed studies to quantify the second characteristics of laser induced plasmas created with micro-, nano-pico- and femtosecond lasers of multiple

#### designs and capacities

These studies will examine the characteristics of

In the studies described below, we will describe investigations that explore the human effects of LIP. Studies are proposed to determine the capacity of to evoke pain. These studies will be performed, *in vitro*, where the factors such as distance and orientation can be tightly controlled, and where the appropriate pain system components can be isolated for detailed quantitative study. A portion of the investigations will apply to sensory cell preparations. These will be generated by conventional means. Subsequent studies will use laser-induced plasmas to create the characteristics of which will be well defined and optimized to produce atraumatic sensory influences.

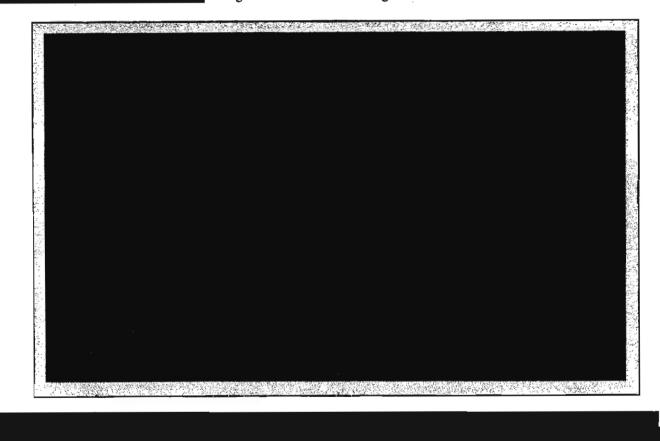
Objective 1: To determine the features that activate nociceptors and the extent to which this activation is effective without trauma. Pain is a primary component of all NLW. Pain can distract and deter individuals resulting in voluntary immobilization and/or flight. Nociceptors are the fundamental detection component of the pain system. Nociceptors transduce a variety of stimuli (gated ionic current) and then encode the pain signal (action potentials). While the mechanisms are not fully understood, ADS operates mainly on the *transduction* component by heating biological tissue to activate heat transducing proteins at a sub-traumatic level (B. Cooper, Microwave Techniques for Stimulation of Nociceptors, NTIC proposal, October, 2003). In contrast, **the section of the section** could activate nociceptors at the level of

encoding, thereby bypassing the transduction level. Induction at the encoding level is potentially more advantageous, as it avoids the direct heating of tissue and the risk that occurs from this time dependent event. Moreover, by engaging the encoding event, will not rely solely on specialized transduction proteins that are selectively expressed in a subpopulation of sensory afferents. Although they differ in isoform and distribution, the proteins that mediate encoding are present in all excitable tissue. In objective 1, we will determine the influence for activation on nociceptor activation, focusing specifically on cutaneous nociceptors that innervate superficial skin (epidermis) and underlying tissue (dermis). The strength required to induce activation, the contribution of pulse duration and burst frequency will be defined in tightly

controlled experiments, *in vitro*. These data should prove to be very useful in interpreting the potential human effects of LIP, and its potential as a NLW.

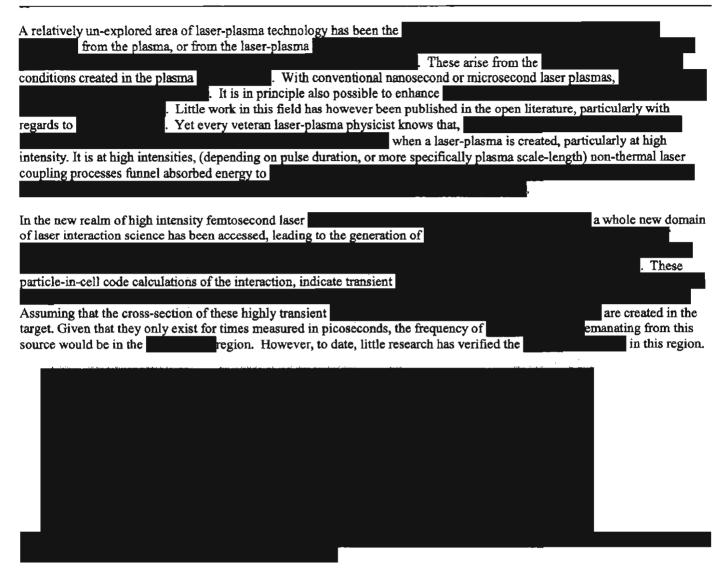
Objective 2: To examine the influence of **sector and a set of a se** 

identical recording methods (but laser stimulation) we will examine the nociceptor activating properties of laser configuration and stimulation regimes.



## **B)** Background

Laser Plasma Technology. There is increasing interest in the use of lasers for non-conventional defense applications. This is not only a consequence of the recent heightened sensitivities in such areas as homeland security, defense force protection, and law enforcement, but it also comes from new technical opportunities becoming available through the increasing pace of developments in laser technology. Developments in solid state laser technology in particular are leading these advances. Diode-pumping, for instance, for the first time enables electrical pump energy to be selectively channeled to specific laser transitions within solid-state laser media, leading to vast improvements in laser efficiency, compactness and stability. New evolutions in laser architecture, like fiber-lasers, slab-laser amplifiers, active phase control and ultra-short pulse technology are rapidly opening up new parameter space in sciences and technologies having possible relevance to new defense applications. One of these areas is the field of laser plasmas.

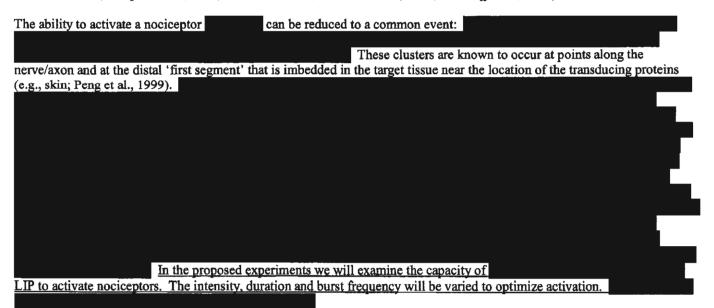


There is extensive interest in developing weapons systems that utilize pulse energy projectiles (PEP). When appropriately configured, a PEP could serve both lethal and non-lethal applications. The guiding hypothesis of this proposal is that the creation of LIP could serve be a NLW by activation of nociceptors.

The Peripheral Pain System. The detection of pain begins with a complex set of peripheral afferents (nociceptors) that detect and encode a great variety of stimuli. These peripherally encoded events are relayed by axons into the central nervous system (spinal cord, thalamus, cortex) where the information undergoes the complex assembly required to produce a localized, conscious perception of pain (Cooper and Sessle, 1993). Nociceptive afferents detect tissue damaging or near tissue damaging consequences of mechanical and thermal events, and the chemical events associated with actual tissue damage. To accomplish these multilevel tasks, the pain system has evolved a family of nociceptive neurons with diverse mechanical, thermal and chemical response capacities. These capacities overlap in a manner that is not completely understood, but it is likely that they vary for particular tissue sites (skin, joints, muscle, viscera, bone) that have highly specialized nociceptive requirements. Recent advances in nociceptor characterization have permitted classification, in vitro, of at least 8 distinct nociceptive phenotypes. Our laboratory has shown that sensory cells of the DRG are comprised of discrete, internally homogenous, classes of capsaicin (OC) sensitive (types 1, 2, 5, 7, 8 and 9) and insensitive (types 3, 4, 6) populations with distinct capacities to respond to 5HT, PGE<sub>2</sub>, protons, ACh and ATP (Martenson et al., 1994; Cardenas et al., 1997; Cardenas et al., 1999; Petruska et al., 2000, 2002; Cooper and Cooper, 2001). We have used lipid soluble fluorescent tracers to define the specific distribution of nociceptors into viscera, joints and skin. Preliminary studies have indicated that nociceptive populations of skin include types 1, 2, 4 and 5. It is these nociceptors that are likely to receive the maximal burst from laser plasmas

The capacity of a nociceptor to detect and transduce noxious stimuli (heat, mechanical, chemical) is due to the presence of membrane imbedded proteins which act as transducers. Specific proteins have evolved which alter conformation in the . This altered conformation gates a pore to allow ions to pass along their presence of heat, chemical agents, clectrochemical gradients. Microwave radiation, via its capacity to heat tissue, is likely to interact with certain heat sensing proteins that are differentially expressed in nociceptor subpopulations (TRPV1, TRPV2; Caterina et al., 1997, 1999; Tominaga et al., 1998). Such proteins are likely to be the ultimate targets of ADS millimeter wave radiation. In addition to detection and transduction of noxious events, nociceptors, like all sensory afferents must encode the event so that it can be relayed to the central nervous system where perceptions are formed. Each nociceptor emits a code in the form of a series of action potentials that are produced in a frequency that is in proportion to the ionic current of the transduced event. The action potential code arises from the influence of the ionic current on clusters of voltage-gated channels. This can be thought of as an analog to digital conversion, where the ionic current is the analog signal that is converted to a digital code by the cluster of voltage gated channels. This cluster is composed mainly of voltage gated  $Na^+$ ,  $K^+$  and  $Ca^{++}$  channels. Each channel is composed of multiple proteins that form an ionic pore in the neuronal membrane and contain a distinct voltage-sensing region. Sensitivity to internal voltage varies considerably in sensory systems due to the differential distribution and multiple isoforms of voltage gated channels. Voltage gated Na<sup>+</sup> channels (Na<sub>v</sub>) are responsible for the upstroke of the action potential while voltage gate K<sup>+</sup> channels  $(K_v)$  are responsible for the downstroke. Multiple forms of Na, and K, have evolved to set characteristic frequency response rates in different afferent populations. Nociceptors contain multiple forms of these channels (Na, 1.7, 1.8 and 1.9; Fang et al., 2002; Djouhri et al., 2003a,b).

Those Na<sub>v</sub> subtypes that are mainly found in nociceptors (Na<sub>v</sub>1.8 and Na<sub>v</sub>1.9) have relatively high thresholds and slow kinetics. Due to the ultra slow kinetics of Na<sub>v</sub>1.9, only Na<sub>v</sub>1.8 participates directly in action potential generation (Elliott and Elliot, 1993; Akopian et al., 1996; Tate et al., 1998; Cummins et al., 1999; Dib-Hajj et al., 2002).



#### C) Technical Approach and Methodology

**Overview of Experiments.** The goal of the studies, in year 1, will be: 1) to determine the nano- and micro-pulsed regimes that initiate nociceptor activation; 2) to determine the range of frequency modulation of the nociceptive signal that can be produced; 3) to determine the differential influence on distinct skin nociceptor phenotypes; and 4) to determine the point at which trauma might begin to limit the NLW value created. The body of knowledge acquired in year 1 will guide the development of hypotheses regarding the desired features of a plasma for the experiments of year two will test these hypotheses using a variety of lasers

based upon

. Hopefully we will be able to marry these two bodies of knowledge and perfect a laboratory scale NLW laser plasmas.

These studies will be conducted *in vitro*, where nociceptive cells of several phenotypes can be exposed to well specified, intense bursts that simulate exposure to laser **bursts**. Due to methods developed in our laboratory, we are able to identify discrete nociceptive phenotypes that are subpopulations of a large population of sensory cells that mediate touch, proprioception, warmth, cooling, itch and pain sensations (Petruska et al., 2000, 2002). The identified nociceptive subpopulations have been shown to be heat sensitive and thereby involved in the transduction of burning pain sensations (Cooper et al., 2003).

In our studies we will present high intensity **and** nanosecond-micosecond pulses to cutaneous nociceptors (dicarbocyanine dye tracing). These nociceptors express distinct Na, that are likely to manifest differential sensitivity **and** activation. We will determine the threshold for activation for nano- and micro- pulsed **and activation**, the effect of repeated pulsing, pulse duration and intensity. If activation is discrete, we should be able to drive nociceptors in a pulse-by-pulse manner. Alternately, single pulses in these time and intensity domains may not be able to produce any activation. In this instance, burst application that approaches known thresholds of **activation** effectiveness (1 msec) could be used. We will conduct such single, multiple and burst train studies at various power and duration combinations in multiple nociceptive subtypes. We will parallel these studies with examinations membrane damage suggestive of electroporation, cell trauma and death.

Due to limits of the current technology for delivering high **sector** pulses, we will not be able to test in the femto- and picosecond domains in year 1. On the one hand, that will limit our ability to form hypotheses that simplify studies of year 2 involving **sector** single pulse femto- and picosecond lasers. On the other hand, the shorter the duration of the burst, the less likely it will work in single pulse mode. In year 2, **sector** the duration **sector**, these time domains can be examined. We might find that they work in burst mode, where the duration **sector** can be functionally extended into the nanosecond time domain. To that extent, the nanosecond **sector** could successfully emulate a burst of femto- and picosecond laser **sector**. Femto second lasers have logistic advantages over other configurations.

In year 2, we will use our acquired knowledge of pulse duration, frequency and burst regimes to select laser with high promise for NLW effectiveness. Based upon studies using a high repetition-rate (100 Hz) Q-switched Nd: YAG laser and two additional systems that use an open-architecture solid-state oscillator-multi-amplifier system of our own design, we will have determined the characteristics with that best match those

, we will have determined the characteristics that best match those properties we predict (from year 1) will have atraumatic NLW effectiveness. In year 2 we will confirm these hypotheses (adjust as necessary) and examine whether the influence on nociceptors are robust with respect to variations. These variations could include

We will again examine neurons for evidence of damage due to stimulation differ considerably, the methods of recording from cells will remain the same. Because of the use of lasers in year two, the studies will shift to the University of Central Florida site (M. Richardson laboratory). Neural recording equipment will be shipped to the site, and some additional purchases will be made for auxiliary instruments that would be needed at the non-UF location.

Nociceptor Recordings. Conventional whole cell patch recordings would be desirable and could be made in many of the planned experiments. These will always be suitable for classification of nociceptive cells at the beginning of each experiment prior to the application of sectors. These methods may be suitable for recording during single or dispersed sectors. However, as the duty cycle or burst frequency increases, the ability to make such recordings by conventional methods is less likely. Therefore we will plan to use optical methods to assess action potential discharge. Accordingly, cells will be perfused with sensitive dye sensitive dye will be perfused with sensitive dye sensitive dye sensitive dye will be perfused with sensitive dye sensitive dy

All recordings are conducted at 35° C.

Procedures: Nociceptor Activation. Once the whole cell patch configuration is achieved, cells are classified by physiological criteria associated with nociceptors (voltage clamp mode; see Petruska et al. 2000, 2002). The main studies are carried out in current clamp mode. The cell (20-45 um diameter) is centered in the field (eyepiece reticule). The microscope is configured for application by the introduction of a pair of stainless steel plate electrodes that have been pre-positioned to bracket the cell under investigation (3 mm, separation). During recordings, cells are exposed to nano- or microsecond pulses from one of the pulsers . These devices can produce pulse durations from 10 . High exposures are commenced at planned intensities, durations, nanoseconds to 100 microseconds repetition rates, and burst frequencies. Optical recordings are made continuously and captured by software for analysis. Studies will define the minimum field characteristics that produce activation, and then proceed with higher burst frequencies, longer durations and more intense fields to determine the limits of activation and the point at which trauma occurs. Using conventional records, we will monitor RMP at regular 'rest' intervals.

Studies will proceed on a variety of skin nociceptive phenotypes (types 1, 2, 4 and 5). Differences in susceptibility are likely to be observed due to quantitative and differential expression of TTX sensitive channels (Nav1.7 vs Nav1.8). We will use QX314 (5 mM) or TTX (1 uM) to determine whether the dye emissions are due to gating of Nav. or a direct influence of dye emission. Some time limited artifact is expected. If prolonged, false signals are

indicated, we will shift to Ca<sup>++</sup> sensitive dyes. We will also consider thermal contributions by examining the inter-plate temperature shifts associated with stimulation protocols.



Measurement of nano and micro pulsed E fields. We will devise a range of instruments to assess fields generated. These will be developments from devices we have used in the past fields generated, and also devices developed specifically for these studies.

The objective of these measurements will be to:

- Determine the magnitude, time-duration of the plasma, and the from it.
- Analyze the frequency response of the

Several detection systems will be used. Simple single and multiple loop detectors will	be used for measurements
. We have previously used these to measure	from plasmas created by nanosecond
duration long-wavelength, 10 mm, CO <sub>2</sub> laser pulses	We will also use
to examine the fields generated. We will also use more some	ohisticated designs that have
previously been employed to measure weak pulsed signals associated with enviro	onmental protection or defense
applications.	
	Our purpose
here will be to adapt these concepts, and utilize the broad depth of knowledge in	detection

here will be to adapt these concepts, and utilize the broad depth of knowledge in to use with microscopic laser-plasma-based sources.

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# 3. Statement of Work / Deliverables / Milestones

Q 1: TASK 1. Acquisition of equipment, validation of methods
We will determine the stable periods for neural recording and determine the best dye
for optical recording purposes. This quarter also involves training of the post doctoral fellow.
Q2: TASK 2. pulsing of nociceptive neurons
We will determine thresholds and suprathreshold stimulation regimes. We will verify that these
stimulus protocols function via Nav. We will evaluate the contribution of and and cell death
endpoints.
Q3-4: TASK 3. pulsing of nociceptive neurons
We will pursue tests on multiple nociceptive phenotypes. We will evaluate the contribution of
and cell death endpoints.
Q5: TASK 4. Preparation for laser studies
We will move the neural recording rig to UCF. Modifications will be made to the recording rig to make
it laser ready and laser safe.
Q6: TASK 5. Laser <b>Control</b> and nociceptive discharge: Method validation
We will determine threshold and suprathreshold stimulation regimes. We will verify that these protocols
Q7-8: TASK 6 Laser and nociceptive discharge:
We will determine the optimal composition and shape for nociceptor activation
A number of deliverables are anticipated:
a) Experiments will define whether a PEP has NLW capacities by demonstrating the feasibility of nociceptor
activation in vitro
b) Experiments will point to the optimal pulse parameters to evoke peak nociceptor activation
c) Experiments will define the limits of tolerance for PEP exposure (onset of cell trauma)
d) Definition of the optimal parameters and talarman for DED exposure (oliset of cell trauma)
d) Definition of the optimal parameters and tolerance for PEP exposure might point strongly toward development
of one laser system over another (micro-, nano-, femtosecond)
e) Experiments will demonstrate scalability of a PEP to act as an NLW and scalability within the NLW continuum
(i.e., moderate to intense nociceptor activation)
f) Experiments will determine the relative utility of laser targeting
to produce the desired, scalable sensory impact.
(1) If outcomes point strongly to one laser system over another this will have implications for a second with the

- g) If outcomes point strongly to one laser system over another, this will have implications for power and weight requirements and logistical support.
- h) Methodologies will be established to study motor systems or investigate possible countermeasures.